

# **WORKSHOP PRESENTATION**

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# Non-contrast T<sub>1</sub> and T<sub>2</sub> relaxometry characterizes reperfusion injury of acute MI in swine

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From 18th Annual SCMR Scientific Sessions Nice, France. 4-7 February 2015

# **Background**

Reperfusion injury in acute myocardial infarction (MI) results in edema, necrosis, microvascular obstruction (MVO), and intramyocardial hemorrhage (IMH), the latter presents an interesting clinical target. [1] Cardiovascular MRI has been shown capable of characterizing all of these tissue components. Other than MVO, which is currently detected by flow-deficient regions in contrast enhanced imaging, all other tissue components can be identified by T<sub>1</sub> and T<sub>2</sub> (T<sub>2</sub>\*). Theoretically, the byproducts of blood breakdown observed with IMH lead to decreased T<sub>1</sub> and T<sub>2</sub> (T<sub>2</sub>\*). [2] Conversely, free water accumulation (edema) and necrosis lead to increased T<sub>1</sub> and T<sub>2</sub>. [2] Hence, direct and quantitative measurement of relaxation rates is promising in myocardial tissue characterization, avoiding ambiguity typical of weighted images (i.e. T2-weighted spin-echo), undesired signal loss from T2\* (weighted) images or the uncertainty introduced by contrast agent kinetics. Hypothesis: Combined T<sub>1</sub> and T<sub>2</sub> mapping can characterize reperfused MI without contrast agents.

# **Methods**

MI was induced in swine by 1 (N=3) or 2 (N=3) hr balloon occlusion of the LAD after the first diagonal, with MRI 7-9 days post MI (Achieva TX, Philips). Relaxometry: 3D respiratory navigator-gated T<sub>2</sub>-mapping [3]; 2D Breath-hold T<sub>1</sub>-mapping (MOLLI) [4]. Clinical standard: breath-hold black-blood T<sub>2</sub>W TSE (BB-T<sub>2</sub>-STIR) [5]; early (3 min post) gadolinium-enhanced images (EGE) using PSIR and 0.2 mmol/kg Magnevist. [6]. IMH was

identified in  $T_2W$  images/ $T_1/T_2$  maps as areas of hypointensity surrounded by hyperintense signal/ $T_1/T_2$  representing edema. MVO was defined in EGE images as hypointense areas surrounded by enhanced MI. The co-localization of tissue types among techniques was examined.

### **Results**

IMH was detected in all animals with 2 hr occlusions, identified by decreased  $T_1$  and  $T_2$ , and was spatially consistent with the hypoenhanced core in BB-T<sub>2</sub>-STIR and with MVO in EGE. Edema was observed in all animals (elevated  $T_1$  and  $T_2$ ). (Fig. 1)

Planimetry showed that relative to remote myocardium,  $T_1$  and  $T_2$  of edema were significantly higher (p < 0.001 and p <1e-5, respectively), while within IMH  $T_1$  was lower (p = 0.001) and  $T_2$  the same (p = 0.28). (Fig. 2)

## **Conclusions**

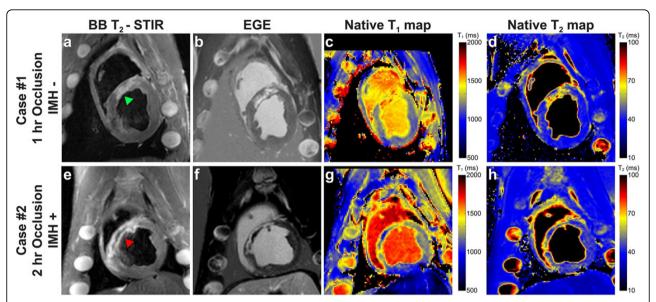
Though either  $T_1$  or  $T_2$  can be used to separate tissues, combined  $T_1$  and  $T_2$  mapping may allow for more accurate detection of IMH in reperfusion injury, without variability from contrast kinetics, or BB- $T_2$ -STIR artifacts. [7] Based on a small number of animals,  $T_2$  was superior in edema detection, while  $T_1$  performed better in IMH detection. Combined relaxometry may identify tissues with better specificity than individual and may help clarify the link between MVO and IMH. High-resolution relaxometry may be necessary to avoid partial volume.

## Funding

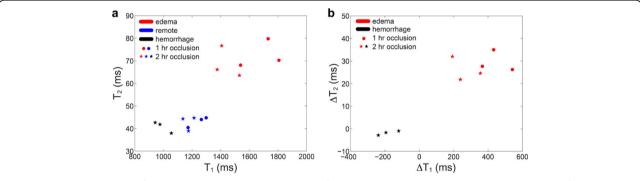
Funded in part by the American Heart Association - 11SDG5280025.

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**Figure 1** Matched representative SAX images from swine without hemorrhage after 1 hr LAD occlusion (Case #1) (a-d) and with hemorrhage after a 2 hr occlusion (Case #2) (e-h). In Case #1, significant  $T_1$  and  $T_2$  elevation are present in both maps (c,d), though no MVO was observed with EGE (b) nor was a hypointense core present in  $T_2$ W images (a). In comparison, Case #2 shows clear IMH, demarked by decrease in  $T_1$  and  $T_2$ , surrounded by edema, shown by increased  $T_1$  and  $T_2$  (g and h), all of which are excellently co-localized with that in  $T_2$ W (e) and EGE (f). Green arrowhead indicates edema; red arrowhead indicates the core of IMH. Note that  $T_1$  mapping is influenced by off-resonance and lower image resolution. As the result of competing effects on  $T_1$  and  $T_2$  from IMH and edema, partial volume averaging makes the  $T_2$  in IMH close to that of normal myocardium.



**Figure 2** a. ROI-based  $T_1 \& T_2$  for edema, IMH and remote myocardium from matched  $T_1$  and  $T_2$  maps. b. Changes in  $T_1 \& T_2$  after subtraction of the reference values of remote myocardium. Edema had higher  $T_2$  than both remote myocardium or IMH.  $T_1$  can be used to discriminate between edema, IMH and normal myocardium, though the distributions may overlap. Edema and IMH can be classified with higher specificity using both  $T_1$  and  $T_2$ .

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#### Published: 3 February 2015

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## doi:10.1186/1532-429X-17-S1-W14

**Cite this article as:** Ding *et al.*: Non-contrast T<sub>1</sub> and T<sub>2</sub> relaxometry characterizes reperfusion injury of acute MI in swine. *Journal of Cardiovascular Magnetic Resonance* 2015 **17**(Suppl 1):W14.